Original Article
Diagnostic utility of fluorogenic peptide-conjugated Au nanoparticle probe corroborated by rabbit model of mild cartilage injury and panel of osteoarthritic patients

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Abstract: Using a rabbit model of early-stage osteoarthritis (OA) and a sampling patients with OA, we evaluated the diagnostic utility of a fluorogenic peptide-conjugated gold nanoparticle (AuNP) probe in detecting mild cartilage injury, based on the a disintegrin and metalloproteinase with thrombospondin motifs 4 (ADAMTS-4) enzyme. Synthesis of this fluorescent turn-on probe (or AU-probe) required conjugation of AuNPs with a fluorescein isothiocyanate (FITC)-modified ADAMTS-4-specific peptide (DVQEFRGVTAVIR). Synovial fluid samples were then collected from 48 adult rabbits and 100 patients for comparative testing (ADAMTS-4 ELISA and AU-probe). Rabbit and patient MRI images were also evaluated and scored. Receiver operating characteristic (ROC) curve analysis was applied to various diagnostic methods (MRI, ELISA, AU-probe, and arthroscopy), performing comparisons via logistic regression. In rabbits, the AU-probe proved nonsuperior to MRI T2 mapping and ELISA (fluorescence cutpoint > 864.965 au). In patient groups, logistic regression analysis indicated that combined AU-probe/MRI testing outperformed MRI alone, thus offsetting low MRI sensitivity and low AU-probe specificity for improved detection of mild cartilage injury (sensitivity, 82.5%; specificity, 80.0%). We have consequently confirmed the efficacy of this AU-probe, using ADAMTS-4 activity in synovial fluid to diagnose mild cartilage injury. Combining the AU-probe with conventional MRI assessment proved optimal in this setting.

Keywords: ADAMTS-4, gold nanoparticle probe, cartilage injury

Introduction

Osteoarthritis (OA) is one of the most common joint disorders, marked by degradation of cartilage and bony remodeling [1, 2]. Typically, it is diagnosed at an advanced stage and cannot be prevented or cured as yet. The degradation of cartilage that takes place at the onset of OA is completely reversible only if the degree of injury is mild [3, 4], which is rarely the case in routine practice. The MRI studies (T1, T2, PD series) customarily performed to evaluate joint cartilage lack the sensitivity to discern mild injury [5]. Although T2 mapping and T1-RHO series are more sensitive in this regard, such tests are time-consuming and device dependent, limiting their application to basic research [6, 7]. Screening of biomarkers associated with injured cartilage by enzyme-linked immunosorbent assay (ELISA) and western blotting is likewise reserved for research purposes, given inherent complexities and time requirements [8]. In this setting, a simple, inexpensive method of diagnosing mild cartilage injury would be ideal.

A disintegrin and metalloproteinase with thrombospondin motif-4 (ADAMTS-4) is an enzyme pivotal in the degradation of aggrecan, which occurs early in cartilage-degrading joint diseases [9, 10]. The aggrecan interglobular domain (IGD) is also cleaved at the Glu373-Ala374 bond [11]. Following the loss of aggrecan, collagen fibrils are degraded, and irreversible tissue failure ensues [12]. A means of gauging ADAMTS-4 activity could thus be useful clinically, enabling early detection of joint degeneration and disease-modifying therapeutic intervention. An
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ADAMTS-4-specific 13-mer peptide, DVQEFR-GVTAVIR (Asp-Val-Gln-Glu-Phe-Arg-Gly-Val-Thr-Ala-Val-Ile-Arg) has been screened previously.

Gold nanoparticles (AuNPs) have special optical properties, including high extinction coefficients and localized surface plasmon resonance (LSPR). Such properties promote the quenching of fluorescence upon exposing fluorescein isothiocyanate (FITC) to AuNPs [13], although fluorescence is restored as FITC and AuNPs are again separated. Moreover, the surfaces of AuNPs are easily modified through strong covalent bonds or physical adsorption based on chemical characteristics. Various studies have reported that the surfaces of

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<th>Group 2 (n = 20)</th>
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<th>Group 4 (n = 20)</th>
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<td>29.3 (19-49)</td>
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<td>27.9 (19-50)</td>
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</table>

Figure 1. Characteristics of AuNPs and AU-probe: (A) TEM images of unconjugated AuNPs (scale bar, 50 nm); (B) TEM images of conjugated AuNPs (scale bar, 50 nm); (C) Distribution of unconjugated AuNPs diameters; (D) Distribution of conjugated AuNPs diameters; (E) Fluorescence intensity curve of AuNP/FITC-peptide conjugate and FITC-peptide only; (F) Statistical comparison of conjugated and unconjugated AuNP diameters; and (G) Fluorescence intensity of AU-probe and AuNPs reacting with pure recombinant ADAMTS-4, respectively.

Schematic 1. Rationale of AU-probe for detection of ADAMTS-4: (A) AuNPs may quench FITC-peptide fluorescence when bonding occurs; (B) For 1 hour, AU-probe reacted with ADAMTS-4; and (C) ADAMTS-4 cleaves aggrecan at E-F bond, with restoration of FITC fluorescence as FITC and AuNPs further separate.
AuNPs may be modified accordingly, using FITC-molecules of proteins or nucleic acid to detect ions, small molecules, and enzymes [14, 15]. Reactive cysteine sulfhydryl groups readily bond to the surfaces of AuNPs, thereby serving as the basis of our research.

In an earlier work, we developed an ADAMTS-4 detective fluorescent turn-on AuNP probe (AU-probe) by conjugating gold nanoparticles with a FITC-modified ADAMTS-4-specific peptide (DVQEFRGVTAVIRC) (Schematic 1) [16]. The present effort was undertaken to establish the diagnostic utility of this AU-probe in osteoarthritic patients and in a rabbit model of mild cartilage injury.

Materials and methods

Preparation of AuNPs and AuNP/FITC-DVQEFRGVTAVIRC conjugate (AU-probe)

AuNPs were synthesized by reduction of HAuCl₄·3H₂O (Aladdin Reagent Inc, Shanghai, China), adding 1.0% HAuCl₄ (0.5 mL) to a reaction flask containing deionized water (47 mL) and heating to 60°C. A mixture of 1% sodium citrate (2 mL; Sigma-Aldrich, St Louis, MO, USA) and 1.0% tannic acid (50 μL; Sigma-Aldrich) was then rapidly added, and the solution was heated to reflux, allowing the reaction to continue (1 min) under uniform and vigorous stirring. In the process, a color change occurred (light yellow → wine red). The AuNP solution was pH-adjusted (7.0) and stored (4°C). AuNP diameters and monodispersity were later examined by transmission electron microscope (Tecnai T20 TEM; FEI [Thermo Fisher], Hillsboro, OR, USA), capturing images (200 kV, 0.35 nm point-to-point resolution). Samples were prepared by pipetting nanoparticulate suspension (10 μL) onto carbon-coated copper grid and allowing the layer (5-50 nm) to settle (20 s), using absorbent tissue to wick away any residual. Image J freeware (National Institutes of Health, Bethesda, MD, USA) helped generate a distribution of nanoparticles by size.

Conjugation of FITC-peptide to AuNPs was achieved as previously reported. Purchased (GL Biochem Ltd, Shanghai, China) FITC-conjugated DVQEFRGVTAVIRC peptide (FITC-Asp-Val-Gln-Glu-Phe-Arg-Gly-Val-Thr-Ala-Val-Ile-Arg-Cys) in solution (1.0 mL; 1.0 mg/mL deionized water) was added dropwise to AuNP solution (10 mL, room temperature) under vigorous stirring for sustained (24 h) reaction. Resultant particles were then washed (three times) with deionized water and stored (4°C). Fluorescence intensity before and after conjugation was assessed using an automatic microplate reader (Thermo Fisher Scientific, Waltham, MA, USA). To gauge conjugate availability, the AU-probe (60 μM) was then reacted with 5 pm pure recombinant ADAMTS-4 (AnaSpec, Fremont, CA, USA) in reaction buffer (50 mM Tris-HCl, 5 mM CaCl₂·2H₂O, 150 mM NaCl, pH 7.5; 100 μL total volume, 37°C, 1 h),
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recording fluorescence data by automatic microplate reader (Thermo Fisher) once the reaction stopped. AuNPs reacted with 5 pm pure recombinant ADAMTS-4 served as control.

Cartilage-injury rabbit model

New Zealand white rabbits (N = 48) aged 4-6 months and weighing 2.5-3.0 kg were procured for this investigation. To create our model of mild cartilage degeneration (for tissue and synovial fluid analysis), we performed medial collateral ligament transection (MCLT) beyond the capsule. Each procedure was conducted as previously described [17], assigning the knees of rabbits to either MCLT (left-sided) or sham (right-sided) groups. Sham procedures were limited to skin incisions (no MCLTs). Eight knees in each group were harvested 2, 4 and 6 weeks later.

High-resolution field emission scanning electron microscope (FESEM) was used to assess microscopic changes of articular cartilage in damaged areas (n = 3). Joint samples (n = 8) were similarly evaluated through MRI studies, including T2 mapping. Mid-medial condyles (n = 8) were also serially sectioned (5 μm) in sagittal plane for histologic processing, staining slide preparations routinely (hematoxylin/eosin [HE]) and selectively (toluidine blue). To assess changes in collagen (types I and II), immunohistochemical staining took place (n = 8). At post-operative Weeks 2, 4 and 6, a normal saline wash (1500 μL) was injected into knee capsules just prior to harvesting. The fluid was then aspirated via sterile knee puncture, removing cells by centrifugation. All samples were stored (-80°C) for later investigation (ELISA and AU-probe).

Patient information and synovial fluid sampling

A total of 100 patients undergoing knee surgery (for meniscus repair, with/without cartilage degeneration) qualified for study (Table 1). Informed consent was obtained in each instance, as stipulated by the ethical review committee of Peking University Third Hospital. Conventional MRI (T1, T2, PD) views of the knee were examined by experienced radiologists and surgeons to assess knee cartilage preoperatively. The Outerbridge classification system was applied to grade MRI (T2) findings as follows: grade 0, intact cartilage; grade 1, signal...
change on T2-weighted MR images; grade 2, defect of cartilage < 50% deep; grade 3, defect of cartilage > 50% deep; and grade 4, full-thickness defect of cartilage with exposed subchondral bone. Highest grades prevailed in instances of multifocal defects. Arthroscopic evaluation was still considered the “gold standard” for assessing deteriorated knee cartilage, again invoking the 5-point Outerbridge scale [18] as follows: grade 0, normal articular cartilage; grade 1, softening or blistering of joint cartilage; grade 2, cartilage fragmentation or surface fissures < 1 cm across; grade 3, cartilage fragmentation/fissuring > 1 cm across; and grade 4, eroded cartilage exposing subchondral bone. The most severe of several injured regions was graded by default.

Patients were ultimately stratified (n = 20 each subset) using the following arthroscopically determined Outerbridge grades: group 0, injured meniscus only (no cartilage defects); group 1, injured meniscus + cartilage (grade 1); group 2, injured meniscus + cartilage (grade 2); injured meniscus + cartilage (grade 3); and group 4, injured meniscus + cartilage (grade 4). Synovial fluid harvested from each group following physiologic saline (20 ml) joint injections were stored (-80°C) in aliquots (100 μL) for subsequent use, limited to one freeze-thaw event only. All procedures were approved by the ethical review committee of Peking University Third Hospital (number IRB00006761-2010085).

**Screening of ADAMTS-4 activity in rabbit and human synovial fluid using probe**

Diluted synovial fluid was incubated with AU-probe (60 μM; 100 μL total volume, 37°C, 1 h). Each sample (100 μL) was then diluted (500 μL) for fluorescence testing. Three synovial fluid aliquots per rabbit or patient were assay-
Enzyme-linked immunosorbent assay (ELISA) of ADAMTS-4 in synovial fluid of rabbits and patients

Levels of ADAMTS-4 in diluted synovial fluid were determined (ELISA kit; Cloud-Clone Corp, Wuhan City, China) per manufacturer’s instructions, expressing results as mean ± standard deviation.

Statistical analysis

The receiver operating characteristic (ROC) curve, area under the curve (AUC), and Youden index were used to gauge accuracy, sensitivity, and specificity of various diagnostic methods. AUC was expressed as mean ± standard error, all other data indicative of mean ± standard deviation. One-way analysis of variance (ANOVA) served to compare patient groups and animal MCLT subsets, assessing differences in sham and MCLT-treated rabbits by independent sam-
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Figure 6. Arthroscopic views of cartilage injury graded by Outerbridge classification (n = 20 per group): (A) Grade 0 (normal cartilage); (B) Grade 1 (softening or blistering); (C) Grade 2 (fragmentation or fissuring of surface, < 1 cm across); (D) Grade 3 (fragmentation or fissuring > 1 cm across); and (E) Grade 4 (cartilage eroded, exposing subchondral bone).

Results

Characteristics of Au nanoparticles (AuNPs) and AuNP/FITC-DVQERGVTAVIRC conjugate (AU-probe)

As noted by TEM, unconjugated AuNPs (mean diameter, 6.96 ± 0.72 nm) were chiefly monodispersed at diameters of ~7 ± 0.5 nm. The AU-probe (FITC-peptide conjugated) remained monodispersed (mean AuNP diameter, 6.99 ± 0.73 nm), showing no significant difference in terms of unconjugated AuNPs. Dispersion of unconjugated AuNP diameters was largely stable at ~7 ± 0.5 nm. Peak fluorescence of the AuNP/FITC-peptide conjugate (AU-probe, 41.25 ± 5.7 au) was vastly weaker than that of FITC-peptide alone (4761.89 ± 358.7 au; P < 0.001). However, the fluorescence observed upon AU-probe reactivity with pure recombinant ADAMTS-4 (2871 ± 176.1 au) proved significantly more intense than that of ADAMTS-4 reacting solely with AuNPs (10.5 ± 2.49 au; P < 0.001) (Figure 1).

Evaluating injury to articular cartilage of rabbits (ultrastructural, MRI, and histologic manifestations)

Ultrastructural changes of articular cartilage were documented postoperatively via SEM. In the sham group, surface cartilage was uniform and smooth throughout the experimental period. By comparison, slight surface unevenness appeared in the MCLT group 4 weeks after surgery, progressing to overtly rough surfaces at 6 weeks in the absence of any fissures (Figure 2).

Conventional MRI and T2-mapping images were both used to evaluate injury of cartilage, which was unapparent by conventional means in both MCLT and sham groups. At 4 and 6 weeks, quantitative changes in T2-mapping images were significantly greater in the MCLT group than in the sham group; and T2-mapping values of the MCLT group at 4 and 6 weeks
were significantly greater than values at 2 weeks (Figure 3).

Histologic features of articular cartilage were examined in HE- and toluidine blue-stained sections. Throughout the experimental period, the sham group was devoid of any apparent degeneration. In the MCLT group, cartilaginous surfaces were intact at 2 weeks, with some fissures detectable at 4 weeks. These fissures increased and deepened by 6 weeks (Figure 4A and 4B). Compared with the sham group, toluidine blue staining weakened at 4 and 6 weeks; and Laverty scores of the MCLT group at 4 and 6 weeks significantly surpassed scores of the sham group (4 W, $P = 0.002$; 6 W, $P < 0.001$). In the MCLT group, Laverty scores of cartilage at 4 weeks were higher than those at 2 weeks postoperatively ($P < 0.001$), and Laverty scores at 6 weeks exceeded those at 2 and 4 weeks postoperatively (6 W:2 W, $P < 0.001$; 6 W:4 W, $P < 0.001$) (Figure 3). Actual Laverty scores are provided in a supplementary table (Supplementary Table 1).

In the MCLT group, staining of type II collagen progressively weakened over time. Between 2 and 6 weeks, the mean density of type II collagen declined dramatically (2 W:4 W, $P < 0.001$; 2 W:6 W, $P < 0.001$; 4 W:6 W, $P = 0.081$), whereas type I collagen showed a significant increase in mean density during the same period (2 W:4 W, $P = 0.004$; 2 W:6 W, $P < 0.001$; 4 W:6 W, $P < 0.001$) (Figure 5).

Evaluating articular cartilage in patients (MRI and arthroscopic Outerbridge grading)

All compartments of the knee joints were evaluated via arthroscopy, assigning 20 patients with meniscus injury only to group 0; 20 patients with meniscus injury and grade 1 cartilage injury to group 1; 20 patients with meniscus injury and grade 2 cartilage injury to group 2; 20 patients with meniscus injury and grade 3 cartilage injury to group 3; and 20 patients with meniscus injury and grade 4 cartilage injury to group 4 (Figure 6).

Outerbridge MRI scores of patients in groups 3 (2.4 ± 0.3) and 4 (3.5 ± 0.32) exceeded those of patients in groups 0 (0.7 ± 0.53), 1 (1.35 ± 0.28), and 2 (2.4 ± 0.74) ($P < 0.001$). In T2 MRI views, injury to cartilage...
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Detection of ADAMTS-4 activity (ELISA) in synovial fluid of patients

ADAMTS-4 concentration in synovial fluid collected from patients of group 0 was less than corresponding levels in groups 1 through 4. In the MCLT group, the ADAMTS-4 concentration in synovial fluid collected at 2 weeks was significantly higher than that collected at 6 weeks ($P = 0.004$) (Figure 8A).

Detection of ADAMTS-4 activity (AU-probe) in synovial fluid of patients

was not evident in patients of group 0 and was difficult to detect in patients of groups 1 and 2 (Figure 7).

Detection of ADAMTS-4 activity (ELISA) in synovial fluid of rabbits

At 2 and 4 weeks after MCLT, the concentration of ADAMTS-4 in synovial fluid showed dramatic increases, compared with levels in the sham group (2 W, $P = 0.006$; 4 W, $P = 0.003$).

Detection of ADAMTS-4 activity (AU-probe) in synovial fluid of rabbits

In the MCLT group, fluorescence recovery of synovial fluid collected at 2 and 4 weeks was significantly higher than in corresponding samples of the sham group (2 W, $P < 0.001$; 4 W, $P < 0.001$). Recovery seen at 2 and 4 weeks clearly exceeded that detected at 6 weeks in rabbits (2 W:6 W, $P = 0.006$; 4 W:6 W, $P = 0.046$) (Figure 9B).

**Figure 8.** Results of patient and rabbit synovial fluid analysis (ADAMTS-4 ELISA): (A) Concentration of ADAMTS-4 in synovial fluid collected from patients of group 0 proved lower than levels in patients of groups 1, 2, and 3 ($P < 0.001$). Mean ADAMTS-4 concentration gradually declined in groups 1 through 4. Average ADAMTS-4 level of patients in group 2 surpassed average levels of patients in groups 3 and 4 (2:3, $P < 0.001$; 2:4, $P < 0.001$); and concentration in group 3 exceeded that of group 4 ($P < 0.001$); and (B) At 2 and 4 weeks after MCLT, ADAMTS-4 concentration dramatically increased, compared with sham group (2 w: $P = 0.006$; 4 w: $P = 0.003$). In MCLT group, synovial fluid ADAMTS-4 concentration at 2 weeks significantly exceeded that found at 6 weeks ($P = 0.004$). No significant difference in ADAMTS-4 concentrations of MCLT and sham groups at 6 weeks postoperatively.

**Figure 9.** Results of patient and rabbit synovial fluid analysis (AU-probe): (A) Fluorescence recovery, nearly undetectable in probe control group, figured prominently in patients of groups 1 and 2, compared with those of group 0 (1:0, $P < 0.001$; 2:0, $P < 0.001$). Fluorescence recovery in patient groups 3 and 4 proved weaker than that encountered in groups 1 and 2 (1:3, $P < 0.001$; 1:4, $P < 0.001$; 2:3, $P < 0.001$; 2:4, $P < 0.001$). Patients in groups 3 and 4 did not differ significantly; and (B) Fluorescence recovery in rabbit synovial fluid collected at 2 and 4 weeks tested significantly higher for MCLT group, compared with sham group (2 weeks, $P < 0.001$; 4 weeks, $P < 0.001$). Synovial fluid samples collected at 2 and 4 weeks showed decisively higher recovery than samples collected from rabbits at 6 weeks (2 W:6 W, $P = 0.006$; 4 W:6 W, $P = 0.046$).
ADAMTS-4 AU-probe for diagnosis of mild cartilage injury

Outcomes of the AU-probe (AUC = 0.804, 95% CI: 0.59-0.94) did not differ significantly from those of T2 mapping (AUC = 0.73, 95% CI: 0.52-0.89; Youden index = 0.50) or ELISA (AUC = 0.73, 95% CI: 0.51-0.89; Youden index = 0.47). At a fluorescence intensity > 864.965 au, mild cartilage injury was detectable (sensitivity, 84.62%; specificity, 63.64%) by AU-probe (Figure 10A). The cutpoint for T2 mapping was at values > 50.1 (sensitivity, 76.9%; specificity, 80.0%). AU-probe, MRI, and ELISA in combination also performed significantly better than MRI alone (AUC = 0.841, 95% CI: 0.724-0.923; P = 0.455).

Accuracy of AU-probe in detecting mild cartilage injury of rabbit model

Outcomes of the AU-probe (AUC = 0.804, 95% CI: 0.59-0.94) did not differ significantly from those of T2 mapping (AUC = 0.73, 95% CI: 0.52-0.89; Youden index = 0.50) or ELISA (AUC = 0.73, 95% CI: 0.51-0.89; Youden index = 0.47). At a fluorescence intensity > 864.965 au, mild cartilage injury was detectable (sensitivity, 84.62%; specificity, 63.64%) by AU-probe (Figure 10A). The cutpoint for T2 mapping was at values > 50.1 (sensitivity, 76.9%; specificity, 80.0%). AU-probe, MRI, and ELISA in combination also performed significantly better than MRI alone (AUC = 0.841, 95% CI: 0.724-0.923; P = 0.455).

Table 2. Receiver operating characteristic (ROC) curve analysis of various test methods applied to rabbit samples

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<th>RABBIT</th>
<th>AUC</th>
<th>SE</th>
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<th>Sensitivity</th>
<th>Specificity</th>
<th>Youden Index</th>
<th>Cutpoint</th>
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<td>0.09</td>
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<td>63.64</td>
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<td>0.11</td>
<td>0.52 to 0.89</td>
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<td>72.7</td>
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<td>0.11</td>
<td>0.51 to 0.89</td>
<td>92.31</td>
<td>54.55</td>
<td>0.47</td>
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AUC, area under the curve; CI, confidence interval; ELISA, enzyme-linked immunosorbent assay; SE, standard error.

Table 3. Receiver operating characteristic (ROC) curve analysis of various test methods applied to patient samples

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<th>SE</th>
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<th>Sensitivity</th>
<th>Specificity</th>
<th>Youden Index</th>
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<td>0.60 to 0.84</td>
<td>97.5</td>
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<td>0.72 to 0.92</td>
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<td>82.5</td>
<td>70</td>
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AUC, area under the curve; CI, confidence interval; ELISA, enzyme-linked immunosorbent assay; SE, standard error.

Figure 10. Results of ROC curve analysis, comparing various diagnostic methods: (A) ROC curves plotted for AU-probe, MRI T2 mapping, and ELISA applied to rabbit model; (B) ROC curves plotted for AU-probe, MRI, ELISA, and combined variables (AU-probe + MRI, MRI + ELISA, and AU-probe + MRI + ELISA); and (C) AUC determinations for AU-probe, MRI, ELISA, and combined variables (AU-probe + MRI, MRI + ELISA, AU-probe + ELISA, and AU-probe + MRI + ELISA). Both AU-probe and MRI in combination significantly outperformed MRI alone (AUC = 0.836, 95% CI: 0.541-0.959; P = 0.035), conferring a sensitivity of 82.5% and specificity of 80.0%. AU-probe, MRI, and ELISA in combination also performed significantly better than MRI alone (AUC = 0.841, 95% CI: 0.724-0.923; P = 0.455).
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Youden index = 0.33) or ELISA (AUC = 0.731, 95% CI: 0.60-0.84; Youden index = 0.53). A fluorescence intensity > 1360.19 au was the cutpoint for detecting mild cartilage injury (sensitivity, 80%; specificity, 65%) by AU-probe. The cutpoint for MRI was at scores > 1 (sensitivity, 47.5%; specificity, 85%), and an ADAMTS-4 concentration > 45.9 was the cutpoint for ELISA (sensitivity, 95%; specificity, 55%).

A combined approach, using both AU-probe and MRI scoring (AUC = 0.836, 95% CI: 0.541-0.959; P = 0.035) significantly outperformed MRI scoring alone, conferring sensitivity of 82.5% and specificity of 80.0% (Figure 10 and Table 3).

Discussion

As shown by patient and animal diagnostics, reflecting ADAMTS-4 activity in synovial fluid, the clinical utility of a fluorescence turn-on AU-probe for detecting mild injury of knee cartilage is no longer in doubt. When combined with conventional MRI, high sensitivity (82.5%) and specificity (80.0%) are achieved.

In our rabbit model of mild cartilage injury, histologic staining helped confirm the extent of cartilage degradation in bony samples. However, use of the AU-probe in animal testing did not prove superior to T2 mapping, thus offering no apparent clinical advantage. Many studies have underscored the merit of T2 mapping in this setting by examining images of type II collagen; but the high cost and lengthy examination times are clinically prohibitive [19, 20]. The efficacy and economy of the AU-probe make it much more suitable as a clinical tool, and its diagnostic sensitivity (84.62%) surpasses that of T2 mapping.

Compared with ELISA, there are four aspects of the AU-probe having more favorable clinical implications. Although ELISA boasts comparatively higher sensitivity (92.31% vs 84.62%), its specificity (54.55%) is quite low. Furthermore, the AU-probe requires much less synovial fluid than ELISA (20 μL vs 100 μL) and is completed in ~1 hour, compared with a 4- to 6-hour time frame for ELISA. Finally, the AU-probe identifies activated ADAMTS-4, a key element in glucosamine degradation, whereas ELISA measures total ADAMTS-4 concentrations, including zymogen content of synovial fluid [16]. Some sources have reported increased mRNA expression of ADAMTS-4 in knee cartilage of patients with late-stage OA [21, 22]; yet in severely affected patients who undergo joint replacement, expression of the inactive ADAMTS-4 proenzyme has been shown to increase, without a commensurate upsurge in activation [23, 24]. Assays of activated ADAMTS-4 are thus more telling than total ADAMTS-4 concentration in depicting the dynamics of OA.

As for the patients we studied, testing of the AU-probe produced similar results. Its diagnostic utility was at least comparable to MRI in determining mild cartilage injury. Despite showing superior sensitivity (AU-probe, 80%; MRI, 47.5%), the AU-probe was lacking in specificity. Nonetheless, logistic regression analysis of combined variables has indicated that dual AU-probe/MRI use yields better diagnostic accuracy than MRI alone (AUC = 0.836, 95% CI: 0.541-0.959; P = 0.035), conferring a sensitivity of 82.5% and 80% specificity. Unfortunately, the same was not true of MRI and ELISA.

At present, a mild stage of cartilage injury (Outerbridge grades 1 and 2) affords the only chance of cure [25, 26]. The AU-probe therefore addresses an urgent need for early OA detection. Based on the specified cutpoint (> 1360.19 au), a diagnosis of mild cartilage injury is achievable in conjunction with conventional MRI studies. The AU-probe provides a means of therapeutic monitoring. Synovial fluid collected during knee surgery or at outpatient clinics may be readily tested, allowing timely adjustments in treatment in line with the status of articular cartilage.

The chief limitation of this study was that all patients showed not only cartilage injury, but also meniscus injury. The latter may equally impact ADAMTS-4 levels in synovial fluid, producing spurious results. Because it was difficult to collect synovial fluid in the absence of other disease, meniscus injury was allowed in the patients we enlisted for our research.

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Disclosure of conflict of interest

None.

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References


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**Supplementary Table 1.** Descriptive statistics for Laverty score at 2, 4 and 6 weeks after surgery

<table>
<thead>
<tr>
<th>Group</th>
<th>Safranin o-fast green</th>
<th>Structure</th>
<th>Chondrocyte density</th>
<th>Cluster formation</th>
<th>Total score</th>
</tr>
</thead>
<tbody>
<tr>
<td>2 W sham of MCLT</td>
<td>0.83 ± 0.41</td>
<td>0.5 ± 0.55</td>
<td>0</td>
<td>0</td>
<td>1.33 ± 0.82</td>
</tr>
<tr>
<td>2 W MCLT</td>
<td>0.67 ± 0.52</td>
<td>0.5 ± 0.55</td>
<td>0.17 ± 0.41</td>
<td>0</td>
<td>1.33 ± 1.03</td>
</tr>
<tr>
<td>4 W sham of MCLT</td>
<td>1</td>
<td>0.17 ± 0.41</td>
<td>0.33 ± 0.52</td>
<td>0</td>
<td>1.5 ± 0.83</td>
</tr>
<tr>
<td>4 W MCLT</td>
<td>4.33 ± 0.52</td>
<td>4.33 ± 0.82</td>
<td>1.67 ± 0.52</td>
<td>0.5 ± 0.55</td>
<td>10.8 ± 1.33</td>
</tr>
<tr>
<td>6 W sham of MCLT</td>
<td>0.67 ± 0.52</td>
<td>0.33 ± 0.52</td>
<td>0.33 ± 0.52</td>
<td>0</td>
<td>1.3 ± 0.82</td>
</tr>
<tr>
<td>6 W MCLT</td>
<td>4.67 ± 0.82</td>
<td>7 ± 0.63</td>
<td>1.67 ± 0.52</td>
<td>1 ± 0.63</td>
<td>14.3 ± 1.03</td>
</tr>
</tbody>
</table>